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Immunostimulatory sutures that treat local disease recurrence following primary tumor resection

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Abstract

Neuroblastoma is a common childhood cancer that often results in progressive minimal residual disease after primary tumor resection. Cytosine–phosphorothioate–guanine oligonucleotides (CpG ODN) have been reported to induce potent anti-tumor immune responses. In this communication, we report on the development of a CpG ODN-loaded suture that can close up the wound following tumor excision and provide sustained localized delivery of CpG ODN to treat local disease recurrence. The suture was prepared by melt extruding a mixture of polylactic acid-co-glycolic acid (PLGA 75:25 0.47 dL g⁻¹) pellets and CpG ODN 1826. Scanning electron microscopy images showed that the sutures were free of defects and cracks. UV spectrophotometry measurements at 260 nm showed that sutures provide sustained release of CpG ODN over 35 days. Syngeneic female A/J mice were inoculated subcutaneously with 1 × 10⁶ Neuro-2a murine neuroblastoma wild-type cells and tumors were grown between 5 to 10 mm before the tumors were excised. Wounds from the tumor resection were closed using CpG ODN-loaded sutures and/or polyglycolic acid Vicryl suture. Suppression of neuroblastoma recurrence and mouse survival were significantly higher in mice where wounds were closed using the CpG ODN-loaded sutures relative to all other groups.

Introduction

The optimal treatment of solid tumors is often surgical resection, but treatment failure is frequently marked by the recurrence of local disease [1]. Neuroblastoma is the most common extracranial solid malignancy of infancy and is a high-risk disease that has a propensity for local recurrence following surgical resection [2]. Following excision of the tumor, the site of resection is closed with biodegradable sutures. Frequent intra-tumoral injections of immunostimulatory cytosine–phosphorothioate–guanine oligonucleotides (CpG ODN) have been shown to be effective in the treatment of neuroblastoma [3, 4]. CpG ODN are potent immunostimulants that have shown potential as adjuvants in a wide variety of diseases including cancer [5, 6]. Here, we report on the development of an immunostimulatory suture that provides sustained release of CpG ODN at the site of tumor excision, so that surgeons can effectively close the wound following removal of the tumor and simultaneously provide local therapy for control and elimination of minimal residual disease.
Methods and materials

Suture preparation
To prepare the immunostimulatory suture, we loaded ground up polylactic acid-co-glycolic acid (PLGA 75:25 0.47 dL g⁻¹, Absorbable Polymers International, Pelham, AL) pellets and CpG ODN 1826 (5′-TCCATGACGTTCCTGACGTT-3′, Coley Pharmaceutical Group, Wellesley, MA) that was endotoxin free (<0.03 Eu mL⁻¹; BioWhittaker, Walkersville, MD) into a Dynisco extruder hopper and sutures were extruded from a melted (≤70 °C) mixture of PLGA pellets and lyophilized CpG ODN. The CpG ODN used in this study has a phosphorothioate-modified backbone that is more resistant to enzymatic and thermal degradation than non-modified CpG oligonucleotides.

Measuring release of CpG ODN from sutures
To characterize the release profiles of CpG ODN, 450 mg of CpG ODN-loaded sutures were placed into 10 mL of phosphate buffered saline (PBS) and placed on a plate shaker at 37 °C. The supernatant was measured for release of CpG ODN at 260 nm on a UV spectrophotometer (Spectramax M5 Microplate reader, Molecular Device) every day and fresh medium replaced.

Scanning electron microscopy
Samples for scanning electron microscopy (SEM, Hitachi S-4000) were prepared by coating suture samples on steel stubs with approximately 5 mm of gold by ion beam evaporation using a sputter coater (E550 Emitech sputter coater) set at 10 mA for 10 s prior to examination in the SEM operated at a 5 kV accelerating voltage.

Murine tumor cell lines
Neuro-2a (N2a), a murine neuroblastoma wild-type cell line, was purchased from American Type Culture Collection (Manassas, VA). The cells were cultured in vitro in minimal essential medium (GIBCO, Grand Island, NY), supplemented with 10% fetal bovine serum (Hyclone, Logan, UT), 1% penicillin–streptomycin (10,000 U mL⁻¹), 10 mmol sodium pyruvate, 100 mmol nonessential amino acid (GIBCO), 0.75 g sodium bicarbonate (Fisher Scientific, Fair Lawn, NJ) and were free of Mycoplasma.

Anesthetic agents and animal care
Female A/J mice (6–8 weeks old; Harlan Laboratories, Indianapolis, Ind) were anesthetized using halothane inhalation (Halocarbon, Rive Edge, NJ) during inoculation. Mice undergoing tumor resection were anesthetized with intraperitoneal ketamine (87 mg kg⁻¹) and xylazine (13 mg kg⁻¹) mixture, and tumors were resected under sterile conditions. All of the animals were housed under standard conditions, which follow the US Public Health Services guide for the care and use of animals. Mice were euthanized if tumor size was greater than 2.5 cm in any dimension or if mice displayed a ‘sick mouse posture’.

Model of minimal residual disease
N2a (1 × 10⁶) wild-type cells were inoculated subcutaneously on day 1. Caliper measurements of tumor development and growth were documented at least three to four times a week, and volumes were calculated as width² × length × 0.5. At a specified time point, when all the tumors had reached between 5 and 10 mm in any dimension, the tumors were resected without lymph node dissection. Mice were randomized before assigning to groups 1–4. The average maximum sizes of the tumors in any dimension for each group prior to resection were (1) 6.3 ± 3.2 mm, (2) 8.1 ± 1.6 mm, (3) 5.9 ± 3.9 mm and (4) 7.4 ± 2.3 mm. The four groups tested included mice that had (1) wounds closed with polyglycolic acid Vicryl suture (Ethicon), (2) wounds closed with Vicryl at which time the site of resection was locally injected with 200 μg CpG ODN, (3) wounds closed with Vicryl and CpG ODN-loaded suture implanted into the same mice remotely on the opposite side to the resection site and (4) wounds closed with Vicryl and CpG ODN-loaded suture.

Statistical analysis
The statistical analyses focused on different wound closure strategies following tumor resection and the effects on tumor recurrence and progression. The primary outcomes of interest were time to death and tumor growth over time. The log-rank test was used to compare the survival times between vaccination groups and Kaplan–Meier survival functions. Tumor size (cm²) was regularly measured throughout the experiments, resulting in repeated measurements across time for each mouse. Mixed linear regression models were used to estimate and compare the group-specific tumor growth curves. Continuous first-order autoregressive structures were specified in the models to account for the within-subject correlation. In both the survival and growth curve analyses, statistically significant global tests of equality across groups were followed up with pairwise comparisons to identify specific group differences.

Results and discussion
Immunostimulatory sutures were prepared by extruding a melted (≤70 °C) mixture of PLGA (75:25 0.47 dL/g) pellets and lyophilized CpG ODN 1826 (figures 1(a) and (b)). Each piece of suture extrudate used in tumor suppression experiments was approximately 0.6 mm × 30 mm in dimensions with an average weight of 150 mg and loaded with 200 μg CpG ODN. Scanning electron microscopy images provided confirmation of the suture dimensions and showed that sutures had a solid morphology with no noticeable fractures or cracks (figure 1(c)). In release studies, CpG ODN was found to be released over 35 days at a sustained rate (figure 1(d)). Release studies were carried out in PBS and we acknowledge that the presence of serum and enzymes found in vivo could alter the overall kinetics of CpG ODN release. However, we anticipate broadly similar sustained release profiles in vivo, as the primary mechanism of PLGA degradation is hydrolytic
Figure 1. (a), (b) Photograph of suture extrudate production. CpG ODN 1826 and ground PLGA pellets (75/25 0.47 dL g⁻¹) are placed into the hopper. At an operational temperature of 70 °C for the rotor, flexible suture material is formed. (c) Scanning electron micrographs show the initial solid structure and the surface morphology of the CpG ODN-loaded sutures (scale bar = 0.4 mm). (d) Release profiles of CpG ODN measured using UV spectroscopy at 260 nm show sustained release of CpG ODN for over a month in PBS (n = 3 ± SD). Images and release profiles are representative of at least two repeats.

Figure 2. Tumor growth (a) and survival (b) of mice inoculated with 1 × 10⁶ wild-type tumor cells. Subcutaneous tumors were grown between 5 and 10 mm following which mice underwent resection of the local disease. The wound at the site of resection was closed and four groups of mice were compared for recurrent tumor growth and survival. Group 1 had wounds that were closed using commercial polyglycolic acid Vicryl suture (n = 10), group 2 was injected with CpG ODN locally and wounds closed using Vicryl (n = 10), group 3 had wounds closed using Vicryl and sutures loaded with CpG ODN were implanted into the same mice remitely on the opposite side of the resection site (n = 10), and group 4, the wounds were closed with Vicryl and CpG ODN-loaded suture (n = 10). Growth curves in each group were compared to each other and to controls. (a) Tumor volume estimates from mixed linear models analysis of the 4 groups of mice. Tumor volume (cm³) is plotted as the mean ± SD. Growth in group 4 was significantly different to all other groups (P < 0.05). (b) Kaplan–Meier plot of the estimated survival functions for the 4 groups of mice. Survival in group 4 was significantly different to all other groups (P < 0.05).

[7, 8]. By controlling the molecular weight and the chemical composition of the PLGA or other biodegradable polymers used to prepare the suture, we can control the release of CpG ODN from weeks to over a year [8–10]. We can control the dimensions of the suture by adjustment of the draw rate which provides a further mechanism for controlling the release profiles and mechanical properties of the suture. Increasing the draw rate decreases the mean diameter of the suture extrudate. The draw rate, composition and molecular weight of PLGA used in the tumor suppression experiments in this study were carefully selected to closely match the duration of tumor growth measurements.

The murine subcutaneous neuroblastoma model is an ideal model for testing the potential use of the immunostimulatory suture as it reliably and aggressively recovers after resection [1]. To evaluate the use of immunostimulatory sutures in preventing recurrence of tumor in the minimal residual disease setting, we tested four groups of mice in which the primary tumor was resected. These groups (described in the materials and methods section) included mice in which the site of excision was then closed using either the immunostimulatory CpG ODN-loaded sutures and/or Vicryl and tumor growth development monitored. All experiments were repeated at least once.

Syngeneic female A/J mice (6–8 weeks old; n = 10 per group; Harlan Laboratories, Indianapolis, IN) were anesthetized using halothane and inoculated subcutaneously with 1 × 10⁶ Neuro-2a (N2a, ATCC, Manassas, VA) murine neuroblastoma wild-type cells on day 1. Tumor growth was measured with calipers and once the tumors had grown between 5 and 10 mm in any dimension, the mice were anesthetized with an intraperitoneal injection of ketamine (87 mg kg⁻¹) and xylazine (13 mg kg⁻¹) mixture and the tumors resected. Figure 2(a) shows that neuroblastoma recurrence and growth were suppressed most significantly in mice in which the excision site contained the immunostimulatory CpG ODN-loaded suture. Prevention of neuroblastoma recurrence
reduced to a minimal residual disease, only to later fall victim to progressive residual disease [1]. These pre-clinical results suggest that closing the tumor excision wound site using CpG ODN-loaded sutures has the potential to result in significant improvements in patient survival rates. Sutures prepared from PLGA are FDA approved and have been used effectively in patients for many years. CpG ODN as an adjuvant is demonstrated to be safe in primate models and in phase 2/3 human clinical trials [16]. The suture preparation uses an extrusion process that is simple, reproducible and adaptable for loading of a wide variety of other anti-tumor molecules, cytokines, antigens and immunostimulants in combination or alone. Immunostimulatory sutures are therefore expected to have significant impact in a clinical setting.

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