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# Chromatic X-ray imaging with a fine pitch CdTe sensor coupled to a large area photon counting pixel ASIC

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ABSTRACT: An innovative X-ray imaging sensor based on Chromatic Photon Counting technology with intrinsic digital characteristics is presented. The system counts individually the incident X-ray photons and selects them according to their energy to produce two *color* images per exposure. The energy selection occurs in real time and at radiographic imaging speed (GHz global counting rate). Photon counting, color mode and a very fine spatial resolution (more than 10 LP/mm at MTF50) allow to obtain a high ratio between image quality and absorbed dose. The individual building block of the imaging system is a two-side buttable semiconductor radiation detector made of a thin pixellated CdTe crystal coupled to a large area VLSI CMOS pixel ASIC. Modules with 1, 2, 4, and 8 block units have been built. The largest module has  $25 \times 2.5$  cm<sup>2</sup> sensitive area. Results and images obtained from testing different modules are presented.

KEYWORDS: Solid state detectors; X-ray detectors; Pixelated detectors and associated VLSI electronics; X-ray radiography and digital radiography (DR)

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### 1 Introduction

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The continuous progress and down-scaling in deep-submicron CMOS technology has allowed to produce ASICs which can integrate hundreds of thousands of full electronic chains (analog frontend and digital counting). Each individual chain is characterized by increasing complexity and functionalities [1–11]. By coupling a custom VLSI pixel ASIC to a thin pixellated CdTe crystal, we have realized an innovative X-ray imaging sensor (PIXIRAD) based on Chromatic Photon Counting technology. The device can produce two '*color*' X-ray images from a single exposure thanks to the double-threshold discrimination system which is capable of counting the photons in two different energy bins in real time.

#### 2 The X-ray imaging sensor

The basic building block of the PIXIRAD imaging system consists of a pixellated solid-state sensor (CdTe) connected to a geometrically and physically matching CMOS readout ASIC by a *flip-chip bonding* technique. The system has therefore a hybrid architecture in which the sensor and readout electronics are manufactured, processed and optimized separately. The individual block is buttable on two opposite sides, therefore several blocks can be placed side-by side minimizing the dead-space between them. The width of the dead-space area (currently set to two pixels) is determined by the width of the high voltage guard-ring built on the radiation sensor.

The CdTe detector (ACRORAD Co., Ltd., Japan) is a pixellated 650  $\mu$ m thick Schottky type diode, which collects electrons on the pixels. The pixels are arranged on a hexagonal matrix with 60  $\mu$ m horizontal pitch and 51.96  $\mu$ m vertical pitch. The radiation receiving side of the CdTe crystal is metalized with a continuous Pt layer while the contacts on the pixel side are made through

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| Atomic numbers                      | 48, 52                               |  |  |
|-------------------------------------|--------------------------------------|--|--|
| Effective atomic number             | 50                                   |  |  |
| Density                             | $5.85 \text{ g/cm}^3$                |  |  |
| Band-gap energy                     | 1.5 eV                               |  |  |
| Relative dielectric constant        | 11                                   |  |  |
| Mean Energy per e-h pair creation W | $\sim 5  eV$                         |  |  |
| Resistivity                         | $10^9 \Omega \mathrm{cm}$            |  |  |
| Electron mobility $\mu_e$           | 1100 cm <sup>2</sup> /Vs             |  |  |
| Electron mean lifetime $\tau_e$     | $3 \times 10^{-6}$ s                 |  |  |
| Hole mobility $\mu_h$               | 100 cm <sup>2</sup> /Vs              |  |  |
| Hole mean lifetime $\tau_h$         | $2 \times 10^{-6} \mathrm{s}$        |  |  |
| $(\mu \tau)_e$                      | $3.3 \times 10^{-3} \mathrm{cm^2/V}$ |  |  |
| $(\mu 	au)_h$                       | $2 \times 10^{-4} \mathrm{cm^2/V}$   |  |  |

Table 1. The CdTe main characteristics.

the deposition of successive Al/Ti/Au/Ni/Au thin metal films. A negative bias voltage is applied to the sensor using a tiny wire glued in a corner of the top Pt layer. The sensor is characterized by a very low leakage current at 300–400 V when operated at reasonably low temperature (typically  $-20^{\circ}$ C in our case). Table 1 summarizes the main characteristics of the CdTe sensor.

The CMOS ASIC has an active area of  $30.7 \times 24.8 \text{ mm}^2$ . It has been fabricated in  $0.18 \,\mu\text{m}$  CMOS technology using six metal and two poly-silicon layers. The ASIC is organized as a matrix of  $512 \times 476$  hexagonal pixels that match the identical pixel arrangement of the CdTe crystal. The chip integrates more than 350 million transistors. Each pixel pad is connected to a charge amplifier that feeds two discriminators and two 15-bit counters/registers. To reduce unavoidable pixel to pixel DC offset variations on the discrimination level, an auto-zero or selfcalibration circuit has been implemented in each pixel. In this way a single global threshold per discriminator can be applied to the entire matrix. The intrinsic pixel amplifier noise is 50 electrons (rms). This level of electronic noise is achieved by taking advantage of the extremely low pixel capacitance (few fF) and of the relatively long amplifier shaping time (pulse width  $\sim 1 \,\mu\text{s}$  at the base).

The counters are implemented in the form of linear feedback shift registers generating a pseudo-random sequence which uniquely relates the number of events with the 15-bit register content.

During data acquisition, the shift registers are clocked by the trigger generated by their respective discriminators. The pixels in the matrix are organized as 256 column pairs, each column pair having its own controller. In readout mode, the registers of several columns of pixels are serialized under the control of an external clock signal. The serialization of the column pairs is user-programmable: groups of 16, 32, 64 or 128 columns can be built, corresponding respectively to 32, 16, 8 or 4 active data output pads.

Two different data acquisition modes are selectable: dual-threshold mode (2 *colors* mode) or, alternatively, single-threshold continuous reading mode. The latter modality is dead-time free, i.e. it allows counting in one counter while reading the other one.

Table 2 summarizes the main characteristics of the CMOS ASIC.

| Pixel characteristics   |                                 |  |  |
|---|---------------------------------|--|--|
| Shaped pulse duration (at the base)                                       | 1 μs (adjustable)               |  |  |
| Linear range  | > 3000 electrons                |  |  |
|   | (> 15  keV for CdTe, W = 5  eV) |  |  |
| Saturation level  | > 6000 electrons                |  |  |
|   | (> 30  keV for CdTe, W = 5  eV) |  |  |
| Equivalent noise charge (ENC)   | 50 electrons (rms)              |  |  |
| Residual offset after self-calibration                                    | $\pm 30$ electrons              |  |  |
| Dynamic range   | 32768 counts                    |  |  |
|   | (15 bit) per threshold          |  |  |
| Input signal polarity   | positive or negative            |  |  |
| ASIC power consumption  | 3 W                             |  |  |
| Possibility to disable or by-pass pixels                                  | user-selectable                 |  |  |
| Pixel readout   |                                 |  |  |
| Serialization of number of columns for best readout time                  | 16, 32, 64, 128                 |  |  |
| Max readout clock frequency   | 200 MHz                         |  |  |
| Typical readout clock frequency   | 50 MHz                          |  |  |
| Readout time for 32 data outputs = 16 columns serialized                  | 2.4 ms (per counter)            |  |  |
| (16 columns $\times$ 476 pixels $\times$ 15 bits $\times$ 20 ns) @ 50 MHz |                                 |  |  |
| Readout time for 16 data outputs = 32 columns serialized                  | 4.8 ms (per counter)            |  |  |
| Readout time for 8 data outputs = 64 columns serialized                   | 9.2 ms (per counter)            |  |  |
| Readout time for 4 data outputs = 128 columns serialized                  | 18.4 ms (per counter)           |  |  |

Table 2. The CMOS ASIC characteristics.

#### **3** Images and performance

Testing of several configurations of the PIXIRAD imaging system has been performed. Modules with one, two, four and eight PIXIRAD blocks have been assembled. The two pixels dead-space between the blocks is usually removed from the images by off-line interpolation.

The modules are able to deliver clear, highly detailed, noise free X-ray images to be used in medical, biological, industrial or scientific applications over the energy range 1–100 keV. The low energy limit is set by the minimum applicable global threshold, which is 200 electrons.

Images are usually obtained at very high count rate (> 30 GHz for a 4 tile module) by illuminating the samples with radiation from high power medical or diffraction X-ray tubes.

Table 3 lists the main specs of PIXIRAD-1, a single block system with 250 K pixels, 500 K counters and  $3 \times 2.5$  cm<sup>2</sup> active area.

#### 3.1 Chromatic photon counting

Figure 1 shows an example of chromatic photon counting with a single block module, PIXIRAD-1.

Two images of a small gecko are obtained by simultaneously counting the X-ray photons with a low energy threshold, figure 1a, and a higher threshold, figure 1b. Figure 1c shows the image obtained by subtracting the two previous pictures and contains mainly the low energy photons of

| PIXIRAD-1 specs:                       |  |  |  |
|--|--|--|--|
| a single unit Schottky t               | ype CdTe diode (650 µm thick)                    |  |  |
| ASIC + CdTe hybrid block               | $512 \times 476$ pixels                          |  |  |
| Active area                            | $31 \times 25 \text{ mm}^2$                      |  |  |
| Total number of pixels                 | 243712   |  |  |
| Total number of counters               | 487424   |  |  |
| Pixel size                             | $60\mu\text{m}$ with hexagonal arrangement       |  |  |
| Pixel density                          | 323 pixels/mm <sup>2</sup>                       |  |  |
| Pixel rate capability                  | 106 counts/pixel/s                               |  |  |
|  | (dead-time corrected)                            |  |  |
| Global rate capability                 | $2.4 \times 10^{11}$ counts/s (1 chip)           |  |  |
| Pixel dead-time                        | 300 ns   |  |  |
| Position resolution                    | 11 LP/mm at 50% MTF                              |  |  |
| Energy range                           | 1–100 keV  |  |  |
|  | (with pulse height saturation above 30 keV)      |  |  |
| Detection efficiency                   | 100%, 98%, 45%                                   |  |  |
| @10 keV, 50 keV, 100 keV               |  |  |  |
| Counter depth                          | 15 bits  |  |  |
| Readout time at 50 MHz clock           | 5 ms   |  |  |
| Frame rate                             | 200 readouts/s                                   |  |  |
| Minimum applicable global threshold    | 200 electrons                                    |  |  |
| Sensor bias voltage                    | $200 \div 400 \text{ V}$                         |  |  |
| Leakage current density                | 5 nA/cm <sup>2</sup> at 400 V, -20°C             |  |  |
| Typical number of defective pixels     | less than 1%                                     |  |  |
| Number of independent threshold levels | 2 pairs (with possibility of frame by frame fast |  |  |
| (colors)                               | switching between the 2 pairs during exposure)   |  |  |
| Module size (W $\times$ L $\times$ H)  | $14 \times 14 \times 7 \mathrm{cm}^3$            |  |  |
| Module weight                          | < 2 Kg   |  |  |
| Module power consumption               | 60 Watts (mainly used for cooling)               |  |  |
| Module cooling                         | Liquid or forced air                             |  |  |
| Module operating temperature           | $+40 - 40^{\circ}C$                              |  |  |

| Table 3  | Main | characteristics | of t | he PIXIR | AD-1           | unit |
|----------|------|-----------------|------|----------|----------------|------|
| Table J. | wiam | characteristics | UI U |          | $\pi \nu^{-1}$ | unn  |

the incident X-ray beam. Note that the photons in b) are also counted in a), so that the two images are largely correlated and thus no further statistical noise is introduced by the subtraction process.

#### 3.2 Low energy sensitivity

The sensitivity of the PIXIRAD sensors to image low energy X-ray photons is shown in figure 2.

Here, images of a very low contrast object (a jasmine flower) are taken at a global threshold of 200 electrons (corresponding to 1 keV energy, figure 2a) for counter 1, and 1200 electrons (corresponding to 6 keV energy, figure 2b) for counter 2.

For a better visualization of the differences in contrast between the images at 1 and 6 keV thresholds, two different Look-Up Tables (Grays and ICA) are used.



**Figure 1**. Images of a small gecko obtained by simultaneously counting the X-ray photons with: a) a low energy threshold for counter 1 (all photons); b) a high energy threshold for counter 2 (high energy photons); c) subtracting the counts in the pixels of image b) from the corresponding counts in the pixels of image a). The result is a higher contrast, low energy, image.



**Figure 2**. Images of a very low contrast object (a jasmine flower) taken: a) at a global threshold of 200 electrons (1 keV energy, LOW counter), and b) at 1200 electrons (6 keV energy, HIGH counter). Falsecolours are used to improve contrast.



**Figure 3**. Image of a resolution phantom taken with a W anode X-ray tube set at 90 kVp. The plot is a profile across the last two couples of lines on the left. The closest lines are  $50 \,\mu$ m wide with  $50 \,\mu$ m separation.

#### 3.3 High energy sensitivity

The image of a resolution phantom taken with a tungsten anode X-ray tube set at 90 kVp with 2 mm Aluminum filter, is shown in figure 3. The lines are metal strips embedded in a 5 mm thick FR4substrate (vetronite). In the bottom panel of figure 3 is a profile plot taken across the last two couples of lines on the left side. No significant geometrical magnification has been used in the experimental set-up (source-detector distance = 50 cm, object-detector distance = 5 mm). This figure illustrates how the resolving power of the imaging system is good even at such high photon energies and is proven by the capability to distinguish the two closest lines (50  $\mu$ m wide with 50  $\mu$ m separation).

#### 3.4 Spatial resolution

To measure the spatial resolution, a Hüttner type spatial frequency grating (see figure 4a) has been used. The phantom is made of groups of lead bars, whose highest density is 10 line pairs per mm (LP/mm). Figure 4b shows a profile plot across the last four groups of bars including those at 10 LP/mm. At 50% MTF the resolution is 11 LP/mm.



**Figure 4**. a) Image of a Hüttner test object for spatial resolution measurement. b) A profile across the last four sets of bars. The highest density bar pairs (10 LP/mm) are well resolved.

|  | •••••• |
|--|--------|
|  |        |

Figure 5. A single shot X-ray image of a man watch with its leather band taken with PIXIRAD-8.

## 4 PIXIRAD-8, an eight blocks module

The largest PIXIRAD module that has been assembled to date, is a 8 block unit with  $25 \times 2.5$  cm<sup>2</sup> active area. The system has 2 M pixels and 4 M counters.

A single shot X-ray image of a wrist watch with its leather band taken with PIXIRAD-8 is shown in figure 5. The watch is made of plastic and metal parts. The top image (taken at low threshold) better visualizes weakly absorbing materials (plastic, leather) while the bottom image (high threshold) is better to visualize the metal parts.

A prototype system for Digital Mammography realized with the PIXIRAD-8 module, operating in slot-scanning imaging mode, is under development by STM Electronics (Verona, Italy) in collaboration with PIXIRAD in the framework of an R&D project supported by Regione Friuli-Venezia Giulia (Italy).

Digital Mammography is one of the most demanding X-ray imaging applications characterized by very fine position resolution, high sensitivity and DQE [12].

#### 5 Conclusions

The PIXIRAD X-ray sensor is an innovative, high quality, noise free, chromatic imaging system. Its main characteristics are:

- large area of the elementary building block;
- high values of contrast and spatial resolution;
- wide energy range (CdTe radiation sensor);
- high frame rate;
- capability to separate the image in various color components depending on the incident radiation energy;
- capability to operate in dead-time free mode (reading one counter while taking data in the other one).

The presented X-ray imaging system is the technological platform of PIXIRAD Imaging Counters s.r.l., a recently constituted INFN spin-off company (see http://pixirad.pi.infn.it/).

#### References

- M. Campbell, E.H.M. Heijne, G. Meddeler, E. Pernigotti and W. Snoeys, A readout chip for a 64 × 64 pixel matrix with 15-bit single photon counting, IEEE Trans. Nucl. Sci. 45 (1998) 751.
- [2] R. Bellazzini et al., *Direct reading of charge multipliers with a self-triggering CMOS analog chip with 105k pixels at 50 μm pitch*, *Nucl. Instrum. Meth.* A 566 (2006) 552 [physics/0604114].
- [3] X. Llopart, M. Campbell, R. Dinapoli, D. San Segundo and E. Pernigotti, *Medipix2: a 64-k pixel readout chip with 55-μm square elements working in single photon counting mode*, *IEEE Trans. Nucl. Sci.* **49** (2002) 2279.
- [4] R. Ballabriga, M. Campbell, E.H.M. Heijne, X. Llopart and L. Tlustos, *The Medipix3 prototype, a pixel readout chip working in single photon counting mode with improved spectrometric performance, IEEE Trans. Nucl. Sci.* 54 (2007) 1824.
- [5] B. Henrich et al., *PILATUS: a single photon counting pixel detector for X-ray applications*, *Nucl. Instrum. Meth.* A 607 (2009) 247.
- [6] R. Dinapoli et al., *EIGER: next generation single photon counting detector for X-ray applications*, *Nucl. Instrum. Meth.* A **650** (2011) 79.
- [7] P. Delpierre et al., XPAD: a photons counting pixel detector for material sciences and small-animal imaging, Nucl. Instrum. Meth. A 572 (2007) 250.

- [8] X. Llopart, R. Ballabriga, M. Campbell, L. Tlustos and W. Wong, *Timepix, a 65k programmable pixel readout chip for arrival time, energy and/or photon counting measurements, Nucl. Instrum. Meth.* A 581 (2007) 485.
- [9] P. Bartl, T. Michel, F. Nachtrab, N. Uhlmann and G. Anton, *Evaluation of X-ray phase-contrast imaging with the Medipix*, *Nucl. Instrum. Meth.* A 633 (2011) \$143.
- [10] R. Accorsi et al., MediSPECT: single photon emission computed tomography system for small field of view small animal imaging based on a CdTe hybrid pixel detector, Nucl. Instrum. Meth. A 571 (2007) 44.
- [11] J. Jakubek et al., *CdTe hybrid pixel detector for imaging with thermal neutrons*, *Nucl. Instrum. Meth.* A 563 (2006) 238.
- [12] G. Blanchot et al., Dear-Mama: a photon counting X-ray imaging project for medical applications, Nucl. Instrum. Meth. A 569 (2006) 136.